

# Advances in Novel Drug Delivery Strategies for Targeting Brain Tumors: An Insight

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## Review Article

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## ABSTRACT

The development of a drug delivery strategy that can not only cross the Blood Brain Barrier (BBB) rapidly but also target the glioma and reach the core of the glioma is essential and important for glioma treatment. A targeted drug delivery system is a unique approach for drug delivery to the appropriate site which is highly efficient, biocompatible and non-immunogenic. Receptor-mediated endocytosis is one of the targeting approaches, especially for targeting anticancer drugs to cancerous sites. In the brain, cancer cells have overexpressed receptors like folate, transferrin, low-density lipoprotein, and hyaluronic acid receptors which can be used for effective site-specific drug delivery to cancerous cells using appropriate receptor-specific ligands. Active and passive targeting promotes tumor specificity with reduced possible side effects. Several nanocarriers like liposomes, nanoparticles, micelles, and dendrimers are used in the delivery of drugs to the target site. There is many transporter also involves in targeting. Targeted drug delivery systems have numerous clinical and diagnostic applications. Modern approaches like ligand-mediated or stimuli-sensitive drug delivery systems have been used for the development of multifunctional nanocarriers that can effectively target cells and cellular organelles.

**Keywords:** Targeting; Ligand; Receptors; Cancer; Nano carriers; Blood-brain barrier

## INTRODUCTION

In the last many years, pharmacists and biochemicologists have been involved in research to deliver drugs to the brain at an effective concentration. The major problem for the delivery of anticancer drugs to the brain is the Blood-Brain Barrier (BBB). The presence of a tight junction of brain capillary endothelial cells that abolishes aqueous paracellular pathways across the cerebral endothelial cells, Prevents the free diffusion of solute into the brain. The diffusion or permeability of a drug also depends on its lipophilicity and, therefore, practical strategies are required for the mediating of drug transport across the BBB.

A targeted drug delivery system is referred to as a system having selective and effective localization of drug molecules at target(s) site at therapeutic concentration, but controlling its access to non-target site leading to enhancement of therapeutic effect and reduction in toxicity. Targeted drug delivery systems describe the presence of the drug-carrier complex which delivers the drug(s) completely to the pre-identified target cell in a specific manner. Various approaches have been used either to regulate the distribution of drugs by incorporating them into a carrier system. A receptor is the main target in the case of a targeted drug delivery system which includes its interaction with ligands for site-specific drug delivery. The targeting is highly significant if the target organ has different characteristics than the other parts of the body which leads to the placement of the active drug in the vicinity of the target site and a limiting quantity of drug in the non-target site which minimizes the toxic effects of the drug [1]. The specific characteristic of targeting is the specific drug receptor binding and rate of controlled drug release. A targeted drug delivery system is generally used in cancer chemotherapy. The pathophysiology of cancer cells is different from the normal cell which is a key point for targeting cancer cells. Cancer cells overexpress many receptors which can be used as a suitable target to deliver cytotoxic agents into tumors [2]. The special characteristic of cancer cells has an Enhanced Permeability Retention (EPR) effect which is a selection criterion for the accumulation of nanocarrier in the tumor microenvironment and delivery of the chemotherapeutic drug to the tumor site [3,4]. Several nanocarriers are mainly focused on targeted drug delivery approaches for the active targeting of nanocarriers to tumor sites. The endothelial gaps present between the vascular capillaries play a crucial role in the accumulation of nanocarriers in cancer cells [5].

## LITERATURE REVIEW

### Overexpressed receptors on brain cancer cell

Many cancer cells overexpress various receptors which provide opportunities to understand cancer biology and its management. These overexpressed receptors may be managed by using antibodies or ligands. These ligands do not deliberately interfere with receptor function but exploit receptor overexpression for the targeted delivery of suitable anticancer drugs which cannot distinguish between cancers cell and normal cells. These carrier systems containing the anticancer drugs can directly link with ligands besides such overexpressed receptors present in cancer cells [6]. Recently various ligand-conjugated novel drug delivery systems like liposomes, micelles, dendrimers, quantum dots, carbon nanotubes, etc. have been synthesized for targeted drug delivery to cancer cells [7].

### Receptors used for brain cancer targeting

**Folate Receptor (FRs):** Folate (folic acid) is a high-affinity ligand that maintains high affinity towards folate receptor upon derivatization through its carboxyl-terminal region due to its overexpression in tumor cells [8]. The folate receptor is the

most commonly overexpressed in cancer cells. The folate receptors are present in three isoforms i.e.  $\alpha$ ,  $\beta$ , and  $\mu$  each of which has its tissue-specific distribution in the human body. Folate Receptor  $\alpha$  (FR $\alpha$ ) is a cell surface glycosylphosphatidylinositol-anchored glycoprotein that can be bound with folates *via* receptor-mediated endocytosis. Most of the normal tissues lack the expression of FR- $\alpha$  isoforms except certain epithelial cells of normal tissues which express FR- $\alpha$  where it is isolated by blood circulation. In most of the epithelial lineage of malignant cells of ovarian tumors-  $\alpha$  overexpression is observed in 90% of cases [9]. The FR- $\alpha$  and FR- $\beta$  are closely associated in function and sequence but distinct in cellular specificity and tissue dissemination. Various studies have reported that FR- $\alpha$  was overexpressed in solid tumors such as breast cancer, ovarian cancer, renal cancer, cervical cancer, lung cancer, and endometrial cancer but FR- $\beta$  was expressed predominately in hematopoietic cells rather than solid tumors [10]. FR- $\beta$  is referred to as a pro-inflammatory monocyte marker and is also termed tumor-associated macrophages or M2 anti-inflammatory regulatory macrophage marker.

**Transferrin Receptor (TFRs):** Mainly two types of Transferrin Receptors (TFR1 and TFR2 restricted to hepatocytes) are present in humans. The extracellular domain of Transferrin Receptor 2 (TFR2) has 66% similarity with TFR1. The receptor for TFR1 (also known as CD71), is universally expressed at low levels in maximum normal human tissues. TFR2 is another member of the TFR family which is a protein similar to TFR1 but its expression is largely limited to hepatocytes cells. TFR1 is involved in the entry of iron-bound TF into the cell, and progressions into acidic endosomes into the cells by clathrin-dependent endocytosis [11]. In this mechanism, TRF 1 is recycled back into the cell surface and iron enters into the cell. The TRF1 is a type II receptor that dominates the outer cell membrane of cancer cells. Despite its ubiquitous expression; TFR1 is located on malignant cells at levels many times higher than the normal cells and its expression can be associated with the stage of cancer progression. This highly expressed receptor is involved in the uptake of iron into the malignant cells for cancer cell proliferation which makes them suitable for the targeting of cancer [12].

**Low-density lipoprotein receptor:** The Low-density Lipoprotein Receptor-Related Protein LRP 1 (also known as CD91), a multifunctional endocytic and cell signalling receptor is expressed on the surface of multiple cells such as hepatocytes, fibroblasts, smooth muscle cells, astrocytes, macrophages, neurons, and malignant cells. In the emerging *in vitro* and *in vivo* studies it has been illustrated that LRP1 is mainly involved in many processes like tumor genesis and tumor progression, initiation of tumor cell migration and invasion by modifying matrix metalloproteinase (MMP)-2 and MMP-9 expression [13]. It also inhibits cell apoptosis by regulating the insulin receptor, the serine or threonine protein kinase signalling pathway, and the expression of Caspase-3. LRP1-mediated phosphorylation of the extracellular signalling kinase pathway and c-junction N-terminal kinase is involved in tumor cell proliferation and invasion [14]. LRP1 has been down-regulated by microRNA-205 and methylation of LRP1 CpG islands. Recently discovered novel fusion gene LRP1-SNRNP25 promotes osteosarcoma cell invasion and migration.

## Lectin receptor

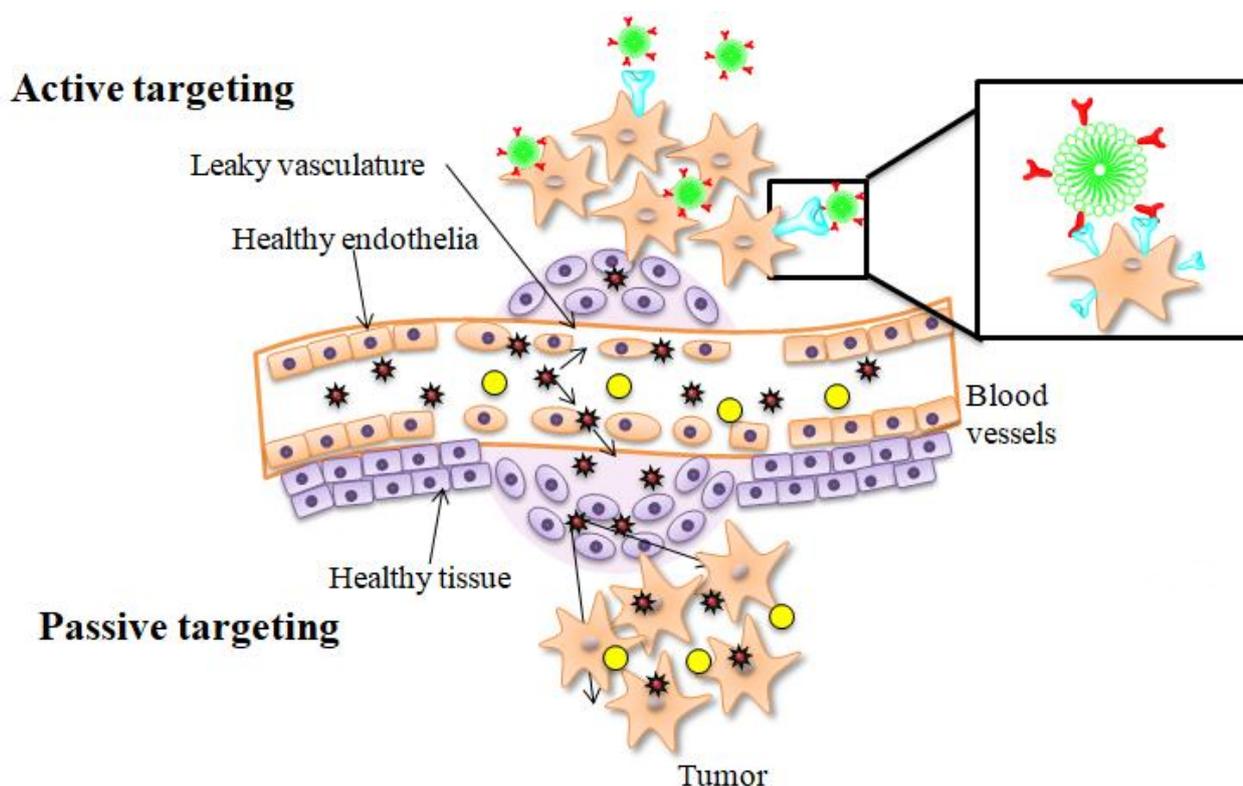
Various lectin receptors are overexpressed in cancer cells in which mannose are the most common receptor. Mannose receptors are the C-type lectin receptors that are expressed on the surface of macrophages and have carbohydrate recognition domains. The mannose receptor responsible for tumor invasion, proliferation, and metastasis in the tumor cells is overexpressed in tumor-associated macrophages. They have potential roles in both innate and adaptive immune

responses and are associated with inflammatory and infectious diseases. Numerous macrophage-targeted liposomes grafted with mannose as a ligand have been developed for cancer treatment [15].

### Strategies for targeting to tumor

Targeted drug delivery may be accomplished by utilization of carrier systems and the various signaling pathways followed by these carriers which protect the drug from bioenvironmental. Drugs targeted especially to cancer cells or specific organelles inside the cells permit the internalization of substances with low cellular permeability by endocytosis and drug release in targeted organelles (e.g., lysosomes, nucleus) [16]. Tumor Micro Environment (TME) is employed as a better target for cancer treatment due to its significant nature in tumor development, progression, and metastasis and also in the development of drug resistance [17,18]. Any modification in TME provides another strategy for the enhancement of penetration of NPs in tumor cells [19]. Tumor micro-environmental conditions which are required for the metastatic cells to survive and proliferate can be exploited for the development of a new therapeutic approach for the treatment of tumors [20,21]. Active and passive targeting of nanocarriers is shown in Figure 1. Various strategies which have been employed in the targeted delivery of tumors are discussed below.

**Figure 1.** Schematic representation of active and passive targeting. **Note:** Receptor, Targeted nanocarriers, Ligand, Small Molecules, Nano carriers, Tumor cell, Endothelial cell.



**Passive targeting:** Passive targeting is referred to as a method to deliver drugs based on the ability of a carrier to circulate for an extended period in systematic circulation [22,23]. Passive targeting occurs because of the body's natural response to the physiochemical characteristics of the drug or drug-carrier system. This type of targeting exploits the natural biodistribution of the carrier system. Passive targeting approaches mainly include the Enhanced Permeability and Retention (EPR) effect, in tumor-bearing organs, and the topical transport of drugs directly to the tumor. Cabral, et al. reported that macromolecules are retained easily in tumors due to the low venous return in the tumor and reduced lymphatic clearance. In passive targeting, the coupling of low MW drugs with a high MW carrier system is inadequately removed by using the lymphatic system of the body and consequently accumulates in tumors. Various types of macromolecules which are permeated by the EPR effect depict wide application potential in cancer drug delivery [23]. The capability of the carrier system occupied by the RES exclusively in the spleen and liver has made them an ideal drug delivery system for hepatic targeting of drugs to these compartments. Nanocarriers are having passive targetability because of the identification of exogenous particulates either in intact or in the opsonized form, by the phagocytic cells of RES.

**Active targeting:** Active targeting is achieved by the modification of drug carriers by receptor-sensitive ligands, which are used for the selective targeting of tumor cells. Active targeting is also known as ligand-based targeting; it is based on ligand-receptor recognition permitting the binding between the ligand and conjugated carriers to the target site [22]. Targeting ligands have been introduced to improve the cell, tissue, and sub-cellular specific delivery through active targeting, as compared to its corresponding non-targeted delivery. Various cell-specific active targeting agents are used to achieve enhanced targeting of cancer-specific cells [24]. Targeting ligands used in active targeting comprises small molecules for example folic acid, peptides (e.g. RGD), proteins (e.g. transferrin), antigen binding fragments (nanobodies) and aptamers [25-30]. There are three levels of targeting-

**First order targeting:** It is referred to as the selective distribution of drug from the carrier system to the desired target site i.e. tissue and organ. It is also known as organ-level targeting or compartmental targeting of the peritoneal cavity, lungs, eyes, etc.

**Second-order targeting:** It is defined as the delivery of drugs to the specific cells of the body. Targeting of tumor cells rather than the normal cell is referred to as second-order targeting. For example the selective targeting of drugs to the kuffer cells of the liver.

**Third order targeting:** It is referred to as the delivery of drugs within the cell component of target cells. The lysosomal degradation of the carrier system is followed by the release of drug intracellularly through receptor-mediated endocytosis which is an example of third-order targeting. Chromatin is a new target and is an area of interest as it provides opportunities for cancer treatment which can show less toxicity than traditional treatments and affects the transcription factor by interfering with the transcription process which is usually a difficult target [31].

**Inverse targeting:** It is a specific type of targeting where the natural RES blockage phenomenon of the body is used. It avoids the passive uptake of the carriers system by the Reticulo Endothelial System (RES) which leads to the reversion of biodistribution of the carrier and hence the process is called inverse targeting. This is based on the suppression of the function of RES by pre-injecting the large amount of blank carrier(s) or macromolecules like dextran sulfate. This leads to the blockage of RES and causes significant impairment of the host defense system [32].

**Dual targeting:** The standard method of drug targeting works on carrier molecules, where the carrier molecules have their intrinsic activity which synergies the pharmacological effects of the loaded drug.

**Double targeting:** In this targeting, the specific drug delivery is achieved by a combination of temporal control and spatial control of drug delivery which leads to a controlled rate of drug release and improved therapeutic effect.

### Transporters responsible for brain cancer

**Monocarboxylate transporter:** Mono Carboxylate Transporters (MCTs) constitute a family of 14 members among which MCT1–4 facilitate the passive transport of monocarboxylates such as lactate, pyruvate, and ketone bodies together with protons across cell membranes. Their anchorage and activity at the plasma membrane require interaction with chaperon proteins such as basigin/CD147 and begin/gp70. MCT1–4 are expressed in different tissues where they play important roles in physiological and pathological processes. This review focuses on the brain and cancer. In the brain, MCTs control the delivery of lactate, produced by astrocytes, to neurons, where it is used as an oxidative fuel. Consequently, MCT dysfunctions are associated with pathologies of the central nervous system encompassing neurodegeneration and cognitive defects, epilepsy, and metabolic disorders. In tumors, MCTs control the exchange of lactate and other monocarboxylates between glycolytic and oxidative cancer cells, between stromal and cancer cells, and between glycolytic cells and endothelial cells. Lactate is not only a metabolic waste for glycolytic cells and a metabolic fuel for oxidative cells, but it also behaves as a signaling agent that promotes angiogenesis and as an immunosuppressive metabolite. Because MCTs gate the activities of lactate, drugs targeting these transporters have been developed that could constitute new anticancer treatments.

**Ion transporter:** Ion transporters are important in the regulation of ionic homeostasis, cell volume, and cellular signal transduction under physiological conditions. They have recently emerged as important players in cancer progression. In this review, we discussed two important ion transporter proteins, sodium-potassium-chloride co-transporter isoform 1 (NKCC-1) and sodium-hydrogen exchanger isoform 1 (NHE-1) in Glioblastomamultiforme (GBM) and other malignant tumors. NKCC-1 is a Na<sup>+</sup>-dependent Cl<sup>-</sup> transporter that mediates the movement of Na<sup>+</sup>, K<sup>+</sup>, and Cl<sup>-</sup> ions across the plasma membrane and maintains cell volume and intracellular K<sup>+</sup> and Cl<sup>-</sup> homeostasis. NHE-1 is a ubiquitously expressed cell membrane protein that regulates intracellular pH (pHi) and extracellular microdomain pH (pHe) homeostasis and cell volume. Here, we summarized recent pre-clinical experimental studies on NKCC-1 and NHE-1 in GBM and other malignant tumors, such as breast cancer, hepatocellular carcinoma, and lung cancer. These studies illustrated that pharmacological inhibition or down-regulation of these ion transporter proteins reduces proliferation, increases apoptosis, and suppresses migration and invasion of cancer cells

These new findings reveal the potential of these ion transporters as new targets for cancer diagnosis and/or treatment.

### Nanocarriers used in cancer targeting

Various nanocarriers have been explored in cancer chemotherapy. Lipid-based nanocarriers and polymeric carriers are extensively employed for targeting cancer cells.

**Nanoparticles:** Nanoparticles (NPs) are a class of materials that include particulate substances which have particle sizes less than 100 nm. NPs are not simple molecules and are composed of mainly three layers (i) The surface layer which may be functionalized with a variety of small molecules, metal ions, surfactants, and polymers (ii) The shell layer which is a chemically different material from the core in all parts (iii) The core which is essentially the central portion of

the NP. Due to such unique characteristics, these materials have the immense interest of researchers in multidisciplinary fields [33].

The pH-responsive multifunctional nanoparticles containing doxorubicin were developed to improve nanoparticle accumulation and drug release in cancer cells by preventing anticancer drug efflux activity. Which conjugation of DOX to the surface of nanoparticles *via* acid-sensitive Schiff-base lead to approximately 6.5-fold improved release at pH 5 versus pH 7.4 in the first 4 hours [34].

**Liposomes:** Liposomes are vesicular systems mainly composed of phospholipids in which an aqueous core is surrounded by lipid bilayers. It can incorporate both hydrophilic and hydrophobic drugs [35]. A pH-sensitive liposomal system containing Tariquidar (TQR); a P-gp inhibitor and Doxorubicin (DOX) was developed to overcome multidrug resistance. It depicted good stability at pH 7.4 and remarkable sensitivity at acidic pH for easier delivery of TQR and DOX. Cellular uptake study evidenced that the liposomal formulations efficiently increased the accumulation of DOX in the nuclei which could be because of raised cellular uptake by P-gp inhibitor TQR. The outcomes revealed that the developed system depicted good potential in the treatment of multidrug-resistant ovarian cancer cells [36].

**Dendrimers:** Dendrimers are monodispersed macromolecules with regular and highly branched three-dimensional structures. Doxorubicin encapsulated PAMAM dendrimers were surface modified with LFC131 peptide which recognized CXCR4 expressed on the surface of breast cancer cells. LFC131-DOX-D4 system improved cytotoxic effect as compared to untargeted DOX-D4 [37,38].

**Niosome:** Niosomes are non-ionic surfactant-based vesicles in which an aqueous core is encapsulated by a nonionic surfactant and cholesterol-assembled bilayer [39]. Tamoxifen Citrate (TMC) encapsulated niosomes were developed as an injectable delivery system for breast cancer therapy. The alteration in the alkyl chain of Spans and the molar ratio of cholesterol controlled the rate of drug release. The results of the In-vitro release study demonstrated prolonged release of drug from niosomes over 7 days. The analysis of cellular uptake and cytotoxic activity was performed in the MCF7 breast cancer cell line. The results revealed 2.8 fold increments in cellular uptake [39].

**Micelles:** Micelles are an aggregate of surfactant molecules dispersed in a liquid with a size range of about 5 nm–100 nm [40]. The Poly (Histidine)-based micelles were synthesized for the delivery of Piperlongumine (PL) and estimated for pro-oxidant anticancer therapy. The PEG-poly(His) micelles improved the loading efficiency of poor water soluble drug (PL). These micelles stimulated the apoptosis process by generation and accumulation of reactive oxygen species and enhanced the cytotoxicity in cancer cells. The folate-conjugated micelles selectively delivered the drug into cancer cells and improved the therapeutic efficacy.

## DISCUSSION AND CONCLUSION

A targeted drug delivery system is an inherent technique for the delivery of drugs to the appropriate sites for effective treatment. Apart from these, it also includes various ligand-mediated drugs targeting with the help of varieties of nanocarriers like liposomes, niosomes, nanoparticles, micelles, and dendrimers which increase the therapeutic effect on the target site with fewer side effects. The lack of thoroughly validated predictive biomarkers has been one of the major hurdles to stratifying cancer patients and monitoring tumor progression and response to the therapy. Investigations in the clinic and preclinical models have provided some molecular and cellular mechanisms for the above challenges. All of these tactics should have their long-term effectiveness and safety taken into account.

Consequently, there are obstacles to be overcome in the delivery of protein or peptide therapies. Various nanocarriers have been developed to overcome these problems. Some of the approaches discussed in this article focused on the safe, easy and efficient delivery of the proteins and peptides of interest. The combination of technologies can be productive for solving the challenges of peptide/protein-based drug delivery in the modern era. Many currently used organic-based drugs are anticipated to be replaced in the very near future by protein and peptide-based medications. To effectively administer these complicated therapeutics in a physiologically active form, the pharmaceutical industry must quickly create workable delivery systems. Their requirement in clinical and therapeutic settings has accelerated research on their practical and efficient noninvasive delivery.

### **CONFLICT OF INTEREST**

All authors declare that they have no conflict of interest.

### **ETHICS APPROVAL AND CONSENT TO PARTICIPATE**

There are no ethical issues the authors need to declare.

### **CONSENT FOR PUBLICATION**

The submitted work has been reviewed and approved by all contributors.

### **AVAILABILITY OF DATA AND MATERIALS**

The present paper has all the data that were produced during this investigation.

### **COMPETING INTERESTS**

The authors declare no competing interests.

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### **AUTHOR'S CONTRIBUTIONS**

Priyanka Bajpai and Om Prakash conducted a literature survey through Science Direct, PubMed, Research Gate, Google Scholar, and various Textbooks wrote, and modified the language such as grammar mistakes, and spelling checking. Amam Mishra generated an idea and revised the manuscript.

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### **REFERENCES**

1. Torchilin V. Tumor delivery of macromolecular drugs based on the EPR effect. *Adv Drug Deliv Rev.* 2011;63:131-135.

2. Jaracz S, et al. Recent advances in tumor-targeting anticancer drug conjugates. *Bioorg Med Chem*. 2005;13:5043-5054.
3. Kale AA, et al. Environment-responsive multifunctional liposomes. *Methods Mol Biol*. 2010;605:213-242.
4. Maeda H, et al. The EPR effect for macromolecular drug delivery to solid tumors: improvement of tumor uptake, lowering of systemic toxicity, and distinct tumor imaging *in vivo*. *Adv Drug Deliv*. 2012; 65:71-79.
5. Deshpande PP, et al. Current trends in the use of liposomes for tumor targeting. *Nanomedicine*. 2013;8:1509-1528.
6. Akhtar MJ, et al. Targeted anticancer therapy: Overexpressed receptors and nanotechnology. *Clinicachimicaacta*. 2014;436:78-92.
7. Bose RJ, et al. Cell membrane-coated nanocarriers: the emerging targeted delivery system for cancer theranostics. *Drug Discov Today*. 2018;23:891-899.
8. Damiani S, et al. Bioinspired detection sensor based on functional nanostructures of S-proteins to target the folate receptors in breast cancer cells. *Sens Actuators B Chem*. 2018;267:224-230.
9. Walters CL, et al. Folate and folate receptor alpha antagonists mechanism of action in ovarian cancer. *Gynecol. Oncol*. 2013;131:493-498.
10. Dhanasekaran S, et al. Augmented cytotoxic effects of paclitaxel by curcumin induced overexpression of folate receptor- $\alpha$  for enhanced targeted drug delivery in hela cells. *Phytomedicine*. 2019;56:279-285.
11. Daniels TR, et al. The transferrin receptor and the targeted delivery of therapeutic agents against cancer. *Biochim Biophys Acta*. 2012;1820:291-317.
12. Voth, et al. Transferrin receptors and glioblastomamultiforme: Current findings and potential for treatment. *J Clin Neurosci* 2015;22: 1071-1076.
13. Feng C, et al. Overexpression of low density lipoprotein receptor-related protein 1 (LRP1) is associated with worsened prognosis and decreased cancer immunity in clear-cell renal cell carcinoma. *Biochem Biophys Res Commun*. 2018;503:1537-1543.
14. Xing P, et al. Roles of low-density lipoprotein receptor-related protein 1 in tumors. *Chin J Cancer*. 2016;35:6.
15. Hagimori M, et al. Synthesis of high functionality and quality mannose-grafted lipids to produce macrophage-targeted liposomes. *Eur J Pharm Sci*. 2018;123:153-161.
16. Minko T, et al. Molecular targeting of drug delivery systems to cancer. *Curr Drug Targets*. 2004;5:389-406.
17. Joyce JA, et al. Therapeutic targeting of the tumor microenvironment. *Cancer Cell*. 2005;7:513-520.
18. Meads MB, et al. Environment-mediated drug resistance: A major contributor to minimal residual disease. *Nat Rev Cancer*. 2009;9:665-674.
19. Chauhan VP, et al. Strategies for advancing cancer nanomedicine. *Nat Mater*. 2013;12:958-962.
20. Psaila B. The metastatic niche: Adapting the foreign soil. *Nat Rev Cancer* 2009;9:285-293.
21. Shi J, et al. Cancer nanomedicine: Progress, challenges and opportunities. *Nat Rev Cancer*. 2016; 17:2-3.
22. Cabral H, et al. Supramolecularnanodevices: From design validation to theranosticnanomedicine. *Acc Chem Res*. 2011;44:999-1008.
23. Thanou M, et al. Polymer-protein and polymer-drug conjugates in cancer therapy. *Curr Opin Investig Drugs*. 2003;4:701-709.

24. Shi JJ, et al. Self-assembled targeted nanoparticles Evolution of technologies and bench to bedside translation. *Acc Chem Res.* 2011;44:1123-1134.
25. Park DH, et al. Biodegradable inorganic nanovector: Passive versus active tumor targeting in siRNA transportation. *Angew Chem Int Ed.* 2016;55: 4582–4586.
26. Z. Jin Y, et al. Core-shell nanocarriers with high paclitaxel loading for passive and active targeting. *Sci Rep UK.* 2016;6:1-6.
27. Guo Y, et al. Transferrin-conjugated doxorubicin-loaded lipid-coated nanoparticles for the targeting and therapy of lung cancer. *Oncol Lett.* 2015;9: 1065–1072.
28. Liu GD, et al. PEG-PLGA Nanoparticle modified by Transferrin Loading Doxorubicin: *In vitro* and *in vivo* Studies for glioma. *Adv Mater Res.* 2013;750–752:1643–1650.
29. Talelli M, et al. Intrinsically active nanobody-modified polymeric micelles for tumor-targeted combination therapy. *Biomaterials.* 2013;34:1255–1260.
30. Hrkach J, et al. Preclinical development and clinical translation of a PSMA-targeted docetaxel nanoparticle with a differentiated pharmacological profile. *Sci Transl Med.* 2012;4:128-139.
31. Peter AJ, et al. Targeting the cancer epigenome for therapy. *Nat Rev Geneti.* 2016;17: 630-636.
32. Shin WK, et al. Cross-linked composite gel polymer electrolyte using mesoporous methacrylate-functionalized SiO<sub>2</sub> nanoparticles for lithium-ion polymer batteries. *Sci rep.* 2016;6:263-268.
33. Daglioglu C, et al. Environmentally responsive dual-targeting nanoparticles: improving drug accumulation in cancer cells as a way of preventing anticancer drug efflux. *J Pharm Sci.* 2018;107:934-941.
34. Torchilin VP. Multifunctional nanocarriers. *Adv Drug Deliv Rev.* 2006;58:1532-1555.
35. Xia Y, et al. pH sensitive liposomes delivering tariquidar and doxorubicin to overcome multidrug resistance of resistant ovarian cancer cells. *Colloids Surf B Biointerfaces.* 2018;170:514-520.
36. Chittasupho C, et al. CXCR4 targeted dendrimer for anti-cancer drug delivery and breast cancer cell migration inhibition. *Eur J Pharm Biopharm.* 2017;119:310-321.
37. Moghassemi S, et al. Nano-niosomes as nanoscale drug delivery systems: an illustrated review. *J Control Release.* 2014;185:22-36.
38. Shaker DS, et al. Cellular uptake, cytotoxicity and in-vivo evaluation of Tamoxifen citrate loaded niosomes. *Int J Pharm.* 2015;493:285-294.
39. Oerlemans C, et al. Polymeric micelles in anticancer therapy: targeting, imaging and triggered release. *Pharm Res.* 2010;27:2569-2589.
40. Hong EJ, et al. Cancer-specific pro-oxidant therapy using low-toxic polypeptide micelles encapsulating piperlongumine. *J Ind Eng Chem.* 2018;63:57-64.